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Crown Ethers: novel permeability enhancers for ocular drug delivery?

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Abstract: Crown ethers are cyclic molecules consisting of a ring containing several ether groups. The most common and important members of this series are 12-crown-4 (12C4), 15-crown-5 (15C5), and 18-crown-6 (18C6). These container molecules have the ability to sequester metal ions and their complexes with drugs are able to traverse cell membranes. This study investigated 12C4, 15C5 and 18C6 for their ability to increase solubility of ocular drugs and enhance their penetration into the cornea. Phase solubility analysis determined crown ethers' ability to enhance the solubility of riboflavin, a drug used for the therapy of keratoconus, and these solutions were investigated for ocular drug permeation enhancing properties. Atomic absorption spectroscopy demonstrated crown ether solutions ability to sequester Ca^{2+} from corneal epithelia and crown ether mediated adsorption of riboflavin into the stroma was investigated. Induced corneal opacity studies assessed potential toxicity of crown ethers. Crown ethers enhanced riboflavin's aqueous solubility and its penetration into *in vitro* bovine corneas; the smaller sized crown ethers gave greatest enhancement. They were shown to sequester Ca^{2+} ions from corneal epithelia, doing so loosens cellular membrane tight junctions thus enhancing riboflavin penetration. Induced corneal opacity was similar to that afforded by benzalkonium chloride and less than is produced using polyaminocarboxylic acids. However, *in vivo* experiments performed in rats with 12C4 did not show any statistically significant permeability enhancement compared to enhancer-free formulation.

Keywords: Crown ethers, corneal epithelium, ocular drug delivery, riboflavin, permeability enhancement, toxicity, *in vitro-in vivo* correlation.

Introduction

Eye drops are generally the preferred means to apply medication when treating ocular disorders; they are convenient and easy to use for most patients. However, this has difficulties despite the fact that the eye is easily accessible since effective drug delivery requires several barriers to be overcome. With aqueous formulations, delivering lipophilic or poorly water soluble drugs at an effective concentration is problematic as is blinking, tear washout and nasolacrimal drainage mechanisms. Up to 90% of the instilled dose is lost almost immediately; more is absorbed systemically to be eliminated by metabolic processes. It is estimated that <1% of the instilled dose penetrates into the eye.^{1,2} When medication is introduced onto the eye there remains only a short time during which the drug can penetrate the cornea.³

Corneal epithelium is a lipophilic structure with tight junctions at the superficial cell layers. This layer offers a resistant barrier which impedes penetration of drug molecules in aqueous solution. However, the underlying stroma, which comprises ~90% of the cornea thickness has a hydrophilic gel-like structure and drugs in aqueous solution easily diffuse throughout this layer.^{3,4}

Keratoconus is a debilitating condition of the cornea which can be treated using riboflavin to initiate ultraviolet 'A' induced collagen cross-linking.⁵ This treatment has become routine practice for the treatment of keratoconus and other corneal disorders.⁶⁻⁹ However, the procedure relies on the physical removal of the epithelium under local anaesthesia to allow stromal penetration of riboflavin.⁵ Developing a means to deliver riboflavin into the cornea without removal of the epithelium would be a significant improvement over the current procedure.

Compounds that are effective at extracting Ca^{2+} ions have been reported to enhance ocular drug permeability.¹⁰ Polyaminocarboxylic acids are a class of compound well known for Ca^{2+}

sequestration¹¹⁻¹⁴ and we have demonstrated this in a recent study using calcium chelators for improved ocular drug delivery.¹⁵

Crown ethers are a class of synthetic macrocyclic polyether molecules first synthesized in the 1960's.¹⁶ With their electron rich hydrophilic cavity due to the lone pairs associated with their oxygen atoms (where cation binding occurs), these molecules have a hydrophobic molecular ring structure, and are able to form guest-host complexes with metal ions and neutral organic molecules. It is thought that these ligands have better affinity to the metal cation on the basis of what fits in the inner cavity. The 'cavity-size' relationship was initially used as the underlying concept to explain binding strength and selectivity and suggested that the binding strength will be highest when the ionic diameter of a cation and the cavity of the crown ether are equal.¹⁷ However, this principle has been revised with the most significant factors now considered to be pre-organisation and complementarity, solvation and chelate ring size.¹⁸ The inherent flexibility of crown ethers allows them to adapt to a range of environments, displaying solubility in aqueous and lipophilic solvents and 'rapid, reversible ion binding characteristics'.¹⁸ According to the Hansch lipophilicity scale, 18C6 has a value of zero, indicating a perfect hydrophilic / lipophilic balance. This is due to the ligand's ability to flex according to the medium it encounters, exposing either hydrophilic oxygen atoms or lipophilic ethylenic groups.¹⁸ This is desirable for ocular drug delivery since the physiology of the eye means that a formulation has to traverse lipid and aqueous phases, and the relatively short residence time means enhancing permeation will allow for greater drug absorption.

Crown ethers have uses in many fields; chemistry, biology, industrial and pharmacological research. Their complexes are able to cross cellular membranes.¹⁹⁻²¹ Crown ethers are used in other therapeutic areas, such as tumour treatment,²² and they have been investigated for

enhancement of drug delivery via vesicular formulations,^{23,24} but as far as we know they have not been investigated for ocular drug delivery. We hypothesized that if these compounds can form complexes with calcium ions they should be able to make the cornea more permeable to drugs by extracting Ca^{2+} , thereby loosening epithelial tight junctions, and their ionophoric properties could assist transit of polyether/drug complexes across corneal epithelium.

In this study we investigated the effects of 3 cyclic polyethers of increasing ethylene oxide units, 12C4, 15C5 and 18C6 for their ability to bind and extract Ca^{2+} and whether they afford any enhancement to the solubility of riboflavin and its corneal penetration. Isothermal titration calorimetry (ITC) was used to analyse their Ca^{2+} binding properties and atomic absorption spectrometry (AAS) employed to determine their ability to extract Ca^{2+} from corneal epithelium. High performance liquid chromatography (HPLC) was employed to determine riboflavin solubility enhancement and *in vitro* experiments using Franz diffusion cells (FDC) to determine drug permeation through whole corneas. Bovine corneal opacity and permeability (BCOP) was used to determine toxicological implications from the use of crown ethers. In vivo experiments were performed in rats, but did not establish any statistically significant ocular permeability enhancement in live animals.

Materials and Methods

Materials. Crown ethers (12C4, 15C5 and 18C6), 2-(*N*-morpholino)ethanesulfonic acid (MES), riboflavin, glacial acetic acid, sodium hexane-1-sulfonate monohydrate, benzalkonium chloride (BAC), ethylenediaminetetraacetic acid (EDTA) and fluorescein sodium salt were supplied by Sigma-Aldrich (Gillingham, UK). Calcium calibration standard (1000 ppm), 10% w/v lanthanum chloride, calcium chloride, potassium chloride, sodium chloride, sodium phosphate, potassium

dihydrogen phosphate, sodium hydroxide (NaOH), hydrochloric acid, optimal cutting temperature compound (OCT), and HPLC grade ethanol were obtained from Fischer Scientific (Hemel Hempstead, UK). Vectashield mounting medium with 4',6-diamidino-2-phenylindole (DAPI) was obtained from Vector Laboratories Ltd (Peterborough, UK). Ultrapure water (18 mΩ cm⁻¹) was used for all aqueous solutions and all materials were used as supplied without modification.

Preparation of buffer solutions

Isotonic phosphate buffered saline (PBS) pH 7.4 ± 0.2, 10 mM 2-(*N*-morpholino)ethanesulfonic acid buffer (MES) pH 7.4 ± 0.2 and 0.005 M sodium hexane-1-sulfonate, pH 3.0 ± 0.2 (ion-pair buffer) was prepared in-house using established protocol. 0.005 M ion-pair buffer for HPLC analysis was prepared by dissolving 1.8822g sodium hexane-1-sulfonate monohydrate to 1800 mL ultrapure water adjusted to pH 3.0 ± 0.2 using glacial acetic acid then made up to 2000 mL with ultrapure water and filtered to 0.2 μm. For isothermal titration calorimetry, 10 mM MES buffer was prepared by dissolving 390.48 mg 2-(*N*-morpholino)ethanesulfonic acid in 180 mL ultrapure water adjusted to pH 7.4 ± 0.2 using 1 M NaOH solution then made up to 200 mL with ultrapure water and filtered to 0.2 μm.^{25,26}

HPLC analysis for in vitro experiments

HPLC analysis was conducted using a Perkin Elmer series 200 system including UV-Vis detector, quaternary pump and autosampler (Perkin Elmer Inc, UK), a 150 mm × 4.1 mm, 10 μm, reversed phase column, part number: 79425 (Hamilton Company, USA) and PeakSimple data acquisition software version 4.09 (SRI Inc, USA). Riboflavin analysis was achieved using the method previously developed by us. Briefly, isocratic analysis over 5 minutes at 25°C, 0.8 mL per minute pre-mixed mobile phase consisting of 20% ethanol and 80% ion-pair buffer, 267 nm

wavelength, 10 μL injection volume and riboflavin retention time of 3.05 minutes. Analysis was quantified against a calibration curve produced from riboflavin standards in PBS, pH 7.4 ± 0.2 with a range of concentrations between 0.01 to 25 $\mu\text{g mL}^{-1}$ ($r^2 = 0.9996$).¹⁵

Atomic absorption spectroscopy

Calcium analysis was achieved using a novAA 350 system with WinAAS software, version 4.5.0 (Analytik JENA, Germany). The analytical method as published by Whiteside and Milner was followed; 50 mm stoichiometric air/acetylene flame, 422.7 nm wavelength, ultrapure water (18 $\text{m}\Omega\text{ cm}^{-1}$) as the carrier.²⁷ Analysis was quantified against a calibration curve produced from aqueous Ca^{2+} standards with 5% lanthanum chloride as a releasing agent. Standards were prepared at concentrations between 0.1 to 10.0 ppm ($r^2 = 0.9921$).

Isothermal titration calorimetry

Ca^{2+} /crown ether binding properties were determined using isothermal titration calorimetry (ITC). A Microcal calorimeter, model ITC200 with software version 1.24.2 (MicroCal Inc. USA). Ultrapure water was put in the reference cell and a reference power of 10 $\mu\text{Cal s}^{-1}$ was selected. 5 mM solutions of crown ethers (12C4, 15C5, and 18C6) in 10 mM MES buffer (pH 7.4 ± 0.2) were titrated by 100 mM CaCl_2 in 10 mM MES buffer. Following the first (redundant) injection at 0.4 μL , 15 further 2 μL injections were made with a spacing of 2.5 minutes and temperature of 25°C. Graphical analysis performed using Origin 7 SR4, v7.0552 software (OriginLab Corporation, USA).

Preparation of animal tissues

Fresh bovine eyes were sourced from a local abattoir (P C Turners, Farnborough, UK) and used within 24 hours after slaughter. Experiments to determine calcium extraction and corneal

opacity experiments employed whole eyes and excised corneas were used for *in vitro* permeability studies using Franz diffusion cells. All experiments were triplicated with a separate eye or cornea used for each repeat.

Whole eye experiments

We have previously reported an experimental technique that we developed to investigate corneal exposure to drug formulations,²⁸ the same protocol was employed in this investigation to determine Ca^{2+} extraction from corneal epithelia. Briefly, individual eyes were placed in beakers, cornea uppermost and packed with loosely rolled up clingfilm to prevent movement, Franz diffusion cell donor compartments were placed over the cornea and held in place by wrapping the whole assembly with clingfilm ensuring a good seal on the eye, the beakers were placed in a water bath at 34 °C. After 10 minutes equilibration the corneas were exposed to aqueous crown ether solutions at either 1 mg mL⁻¹ or 30 mg mL⁻¹ at pH 7.4 ± 0.2. After three hours exposure the solutions were recovered, centrifuged at 10000 rpm (10 g) for ten minutes. Aliquots of each supernatant were diluted by a factor of 100 in 0.25% aqueous LaCl_3 solution for analysis by AAS.

Effect of crown ethers on riboflavin solubility

A series of aqueous crown ether solutions were prepared at 1, 10, 20 and 30 mg mL⁻¹ for each molecular variant, 12C4, 15C5 and 18C6. To each solution an excess riboflavin was added at 1 mg mL⁻¹, and an aqueous solution of saturated riboflavin was used as a control. These solutions were kept in glass vials, wrapped in aluminium foil and stirred overnight at room temperature. Riboflavin saturated solutions were filtered using 0.2 µm Minisart® syringe filters, then diluted with ultrapure water by a factor of 10 for HPLC analysis. Our previous studies have shown riboflavin to be photodegradable,²⁸ and this agrees with data reported by Terekhova *et. al.*²⁹

therefore all experiments and samples were shielded from light using aluminium foil prior to analysis. The association constants of complexation for the crown ethers and riboflavin were calculated using **Equation 1**.

$$K_{a:b} = \frac{slope}{[S_0][1-slope]} \quad (1)$$

Where $K_{a:b}$ is the association constant, S_0 is the intrinsic aqueous solubility of riboflavin and $slope$ is the gradient given by the equation of the graph for riboflavin solubility in crown ether solutions.^{30,31}

Riboflavin solubility enhancement using crown ethers was calculated using **Equation 2**.

$$RF_{Crown} (\%) = \frac{\Delta RF}{RF_{water}} \times 100\% \quad (2)$$

Where $RF_{Crown}(\%)$ is crown ether enhanced riboflavin concentration, ΔRF is the difference between enhanced riboflavin concentration and the intrinsic aqueous concentration of riboflavin and RF_{water} is the intrinsic aqueous concentration of riboflavin.

Effect of crown ethers on riboflavin permeability

Solutions of 12C4, 15C5 and 18C6 crown ethers at concentration of 1 and 30 mg mL⁻¹ in PBS, pH 7.4 ± 0.2 were prepared; riboflavin was added at 0.08 mg mL⁻¹ to dissolve. A solution of riboflavin in PBS, pH 7.4 ± 0.2 was also prepared at the same concentration as a control. Riboflavin permeability was measured using fresh bovine corneas fitted epithelium uppermost in standard Franz diffusion cells (FDC), each cell having an exposed area of cornea of 1.54 cm². 16.5 mL of PBS was placed in the receiving chamber. Prepared FDCs were placed in a water bath, stirred at 34°C ± 1°C to mimic the physiological temperature at the corneal surface.^{32,33} 1

mL of aqueous crown ether solutions, and control was added to the donor compartments which were then covered to prevent evaporation. 0.4 mL aliquots were sampled every hour for 4 hours using sink conditions. Analysis by HPLC was carried out immediately after all samples had been collected to avoid drug degradation. Apparent permeability and steady-state flux were calculated using **Equation 3**.

$$P_{app} = \frac{\Delta Q}{\Delta t \cdot 60 \cdot A \cdot C_0} \quad (3)$$

Where P_{app} is the apparent permeability of riboflavin through bovine cornea, Q is total drug permeated at time t , $\Delta Q/\Delta t$ is the steady-state flux into the receiving solution ($\mu\text{mol min}^{-1}$) which equates to the gradient of the linear portion of the graph, 60 is minutes to seconds conversion factor, A is the area of exposed cornea (1.54 cm^2) and C_0 is the initial amount of drug added to the donor chamber.³¹

Cornea extracts

Crown ether exposed corneas from the riboflavin permeability experiments were trimmed of scleral tissue, blotted dry and placed in vials containing 5 mL absolute ethanol to extract riboflavin. They were wrapped in foil, placed in a box and stored at room temperature for 3 days. After extraction, 1 mL of the extraction solvent was centrifuged for 10 minutes at 10000 rpm (10 g) and the supernatant analysed by HPLC. After riboflavin extraction the corneas were placed in an oven at 40°C overnight to dry and their weight recorded to allow calculation of absorbed riboflavin per mg dry corneal tissue.

Toxicological investigation

Normal cornea's are transparent and impermeable to fluorescein dye due to tight junctions in the corneal epithelium.³⁴ Application of a substance which can denature proteins or cause corneal injury, leading to permeation of the fluorescein dye, reflects toxicological effects to the epithelium. Using a method established in the Bovine Cornea Opacity/Permeability Test ³⁵ (BCOP) described in,³⁴ a scale of epithelial damage and fluorescent intensity was compiled. Corneal opacity and permeability was evaluated using the BCOP test in order to explore toxicological characteristics of crown ethers in comparison to known penetration enhancers and irritants, i.e. benzalkonium chloride and sodium hydroxide. Fresh whole bovine eyes were placed in cups which were subsequently placed in 150 mL beakers, with the corneas facing uppermost. A few drops of PBS were applied to the corneal surface, the beaker was placed in a closed water bath at $34^{\circ}\text{C} \pm 1^{\circ}\text{C}$ and allowed to equilibrate for 10 minutes. A silicon ring was placed on top of the cornea and 0.1 mL of various solutions was applied, including PBS, 18C6 1 and 30 mg mL⁻¹, 15C5 1 and 30 mL⁻¹, 12C4 30 mL⁻¹, EDTA 1 mg mL⁻¹, BAC 0.02%, BAC 0.1%, BAC 0.5%, BAC 1%, BAC 2% and NaOH 0.5M and 1M. The test solution was left on for 30 seconds before being washed off with 10 mL PBS. The beaker was then incubated for a further 10 minutes $34^{\circ}\text{C} \pm 1^{\circ}\text{C}$. The eye was then removed from the beaker and photographed with the silicon ring still in place using a Logitech webcam C920-C, images included in supporting information (**Table S1**). Then 0.1 mL of 2% w/v fluorescein dye solution was placed in the ring and left for 1 minute. The ring was removed and the dye was washed off with 10 mL PBS. The eye was observed under the fluorescence microscope and the fluorescence image was acquired with the exposure set to 130 ms, images included in supporting information (**Table S2**). Both sets of images were processed using ImageJ 1.50b software V 1.8.0_60. Each photograph

was converted to 8-bit images, then the mean grey area function was used to measure opacity for the images, data included in supporting information, (**Table S3**). Fluorescence image data shown in supporting information (**Table S4**). The aim of this experiment was to assess any toxicity of crown ethers in comparison to known irritants, e.g. NaOH, and BAC 0.02% which is often used as a preservative and also as a penetration enhancer in ocular formulations.

In vivo experiments

All in vivo experiments reported in this work were approved by the Ethical committee of Kazan State Medical University (approval no 5 from 28th May 2012). These experiments were conducted with 0.08 mg mL⁻¹ riboflavin solutions with and without 30 mg mL⁻¹ 12C4. These experiments were performed in 3 months Wistar male rats weighting 200-250 g. Animals were housed in stainless steel cages and were fed with a standard multi-ration pellets for rodents (Effect Ltd, Chapaevsk, Russian Federation) and had unlimited access to water. Each formulation was tested in 3 animals. Each animal received 2 mL of the drug solution into both eyes, gradually instilled within 40 minutes. Then animals were sacrificed with a guillotine; both eyes were enucleated using scissors, weighed, quickly washed with 1 mL of 0.9 % saline solution and placed into 1 mL methanol for the drug extraction. Extraction was continued in a refrigerator at 4°C for 24 hours; 0.2 mL of each extract was then mixed with 0.8 mL 0.1 % of aqueous orthophosphoric acid followed by HPLC analysis. Separate experiments were performed to evaluate the retention of sodium fluorescein solutions on corneal surface in rats (n=3). A single drop of 1 mg mL⁻¹ sodium fluorescein solution (~0.05 mL) was administered on rat's cornea; UV light at 254 nm (VL-6.LC, Vilber Lourmat) was briefly shone into their eye to

ensure the dye detection, which under these conditions showed green fluorescence, and digital images were taken immediately and 5 minutes after drop administration.

Histological studies

All histological experiments were conducted similarly to the experiments on *in vivo* administration of riboflavin described in the previous section. Following 40 minutes administration of 1 mL 0.08 mg mL⁻¹ riboflavin solution with and without 30 mg mL⁻¹ 12C4 (n=3), rats were sacrificed with a guillotine; their eyes were enucleated and mounted in OCT and kept on dry ice. Cross-sectioning of each corneal segment was performed on a cryostat (Thermo Scientific Microm HM 525) and fixed on glass slides followed by application of 50–75 µL of 1.5 µg mL⁻¹ DAPI to stain the cell nuclei. Cross sections of rat's cornea were examined using fluorescence microscopy (Olympus BX63); each image was taken using DAPI (blue, maximum $\lambda_{\text{emission}} = 461 \text{ nm}$).

HPLC analysis for in vivo experiments

In order to improve the sensitivity of riboflavin detection in the eye extracts from *in vivo* experiments, a novel HPLC method was developed. HPLC analysis was conducted using a manual injection LC-20 Prominence HPLC system (Shimadzu, Japan) including SPO-20AV UV–vis detector, CTO-20A column oven, LC-20 AD-U solvent manager and Ascentis C18 column, 25 cm × 4.6 mm, 10 µm (part number: 581351-U), and data acquisition software (LCsolution version 1.25). Riboflavin analysis was achieved with a run time of 6 min at 40 °C.

The mobile phase consisted of a mixture of 84 vol % of 0.1 vol % aqueous orthophosphoric acid and 16 vol % acetonitrile, with a flow rate of 1.0 mL min⁻¹, 445 nm wavelength, 10 µL injection volume and riboflavin retention time of 4.9 min. Analysis was quantified against a calibration curve produced from 0.02, 0.03, 0.05, 0.1, 0.2, and 1.0 µg mL⁻¹ riboflavin standards ($r^2 = 0.9994$). The results of these experiments are calculated in µg of riboflavin per 1 g of fresh eye (µg g⁻¹).

Statistical analysis

Minitab® statistical analysis software package, version 16.2.4 was used to analyse data acquired during these experiments using one-way analysis of variance (ANOVA) and paired t-tests. Probability of $P < 0.05$ was considered significant and a minimum of triplicate experiments were used to determine this. Results are reported as the mean \pm standard deviation.

Results and Discussion

Crown ether enhanced aqueous solubility of riboflavin

It was shown that 12C4 at 1 mg mL⁻¹ offered a slight reduction in riboflavin solubility at 0.074 ± 0.003 mg mL⁻¹** compared to the intrinsic aqueous solubility of riboflavin of 0.081 ± 0.004 mg mL⁻¹,^{28,36,37} whilst all other crown concentrations 10, 20 and 30 mg mL⁻¹ enhanced the solubility of riboflavin at 0.088 ± 0.003 , 0.099 ± 0.004 and 0.110 ± 0.004 mg mL⁻¹, respectively.** 15C5 crown ethers at 1, 10, 20 and 30 mg mL⁻¹ all enhanced riboflavin solubility to 0.094 ± 0.002 , 0.104 ± 0.002 ,** 0.109 ± 0.002 ** and 0.118 ± 0.003 *** mg mL⁻¹, respectively, and 18C6 crown ethers at 1, 10, 20 and 30 mg mL⁻¹ all enhanced riboflavin solubility to 0.095 ± 0.003 , $0.100 \pm$

0.003, 0.113 ± 0.003 and 0.115 ± 0.003 mg mL⁻¹, respectively.** * $P < 0.05$ ** $P < 0.005$, *** $P < 0.001$, one way ANOVA, $n = 3$.

From the HPLC results, phase solubility analysis was carried out using the methods developed by Higuchi and Connors (1965)³⁸ and reported by Jarho *et al.* (1996).³¹ Phase solubility plots were produced for mmol L⁻¹ concentrations of the crown ether standards and their corresponding mmol L⁻¹ riboflavin concentration, **Figure 1**.

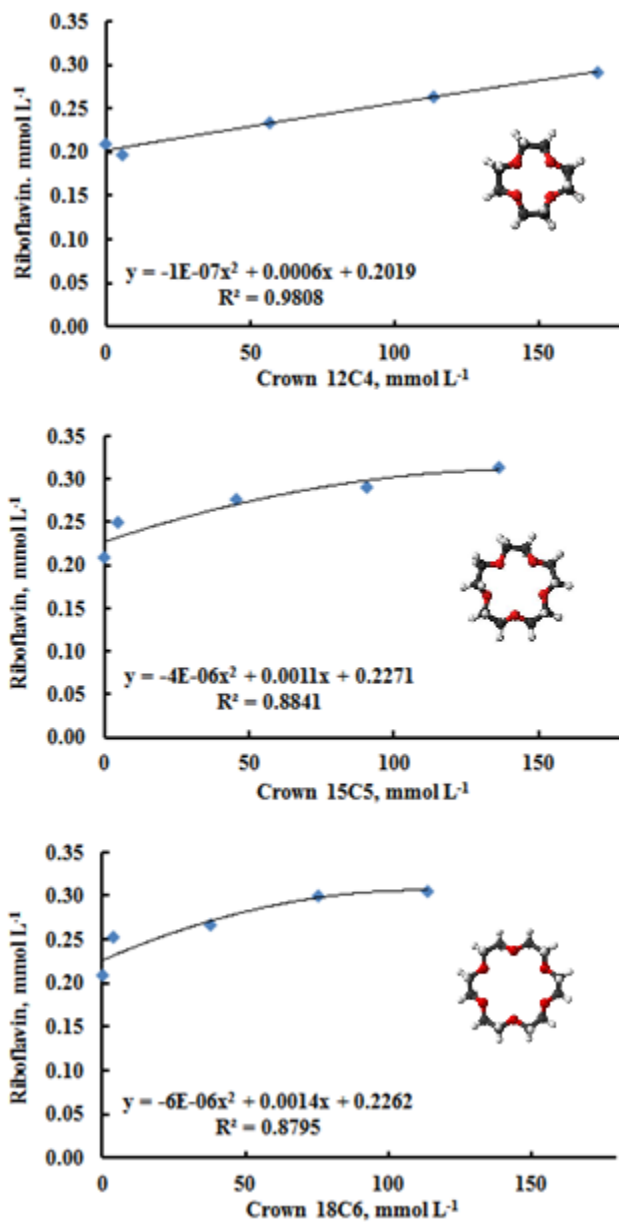


Figure 1 Phase solubility plots for riboflavin / crown ether. Inserts show the structures of 12C4, 15C5 and 18C6.

Crown ether / riboflavin association constants $K_{a:b}$ were calculated using **Equation 1**, and riboflavin solubility enhancement relative to its intrinsic aqueous solubility calculated using

Equation 2. It should be noted that the phase solubility plots for riboflavin with 15C5 and 18C6 are not linear, which introduces some inaccuracy in determination of $K_{a:b}$ compared to 12C4. At 1 mg mL⁻¹ crown ether reduced riboflavin solubility by -9% using 12C4** and enhanced riboflavin solubility by 16% for 15C5** and 17% for 18C6** and at 30 mg mL⁻¹ they enhanced riboflavin solubility by 36% for 12C4,** 46% for 15C5*** and 42% for 18C6.*** **Table 1** lists the concentrations of riboflavin in the various crown ether solutions together with the corresponding association constants and riboflavin solubility enhancement as a percentage relative to riboflavin in deionised water.

Table 1 Crown ether / riboflavin association constant and enhanced solubility compared to riboflavin in de-ionized water.

Crown ether / riboflavin solution	Riboflavin mg mL ⁻¹	Association constant $K_{crown:RF} M^{-1}$	Riboflavin solubility enhancement %
12C4 (1 mg mL ⁻¹)	0.074 ± 0.003	2.39	-9 **
15C5 (1 mg mL ⁻¹)	0.094 ± 0.002	2.87	16 **
18C6 (1 mg mL ⁻¹)	0.095 ± 0.003	3.35	17 **
12C4 (30 mg mL ⁻¹)	0.110 ± 0.004	2.39	36 **
15C5 (30 mg mL ⁻¹)	0.118 ± 0.003	2.87	46 ***
18C6 (30 mg mL ⁻¹)	0.115 ± 0.003	3.35	42 ***

** $P < 0.005$, *** $P < 0.001$, one way ANOVA, $n = 3$.

The trend shows that crown ethers have increasing riboflavin binding affinity and solubility enhancing properties as the molecule size increases. Complex formation depends on the relative size of the host cavity and the guest molecule.^{15,16,39,40} Riboflavin is too large to reside within the cavity of any of the crown ethers investigated in this study,²⁸ however partial complexation is possible and more likely with the larger molecular variants and this could reasonably explain the increasing solubility of riboflavin as larger crown ethers are used. Further studies of the nature of the complexation between crown ethers and riboflavin could potentially be conducted using other techniques, e.g. NMR spectroscopy, but this is outside of the scope of the present work.

Isothermal titration calorimetry analysis of crown ether / Ca^{2+}

ITC was used to determine Ca^{2+} binding efficiency of 5 mM 12C4, 15C5 and 18C6 solutions at physiological pH 7.4. **Figure 2** shows individual raw data and corresponding isotherms of the respective compounds titrated with CaCl_2 . Fitting of the isotherm curves is poorer for crown ethers in comparison with other chelating agent reported by us in a previous study,¹⁵ evident by the lack of any distinct transition seen in the isotherms.

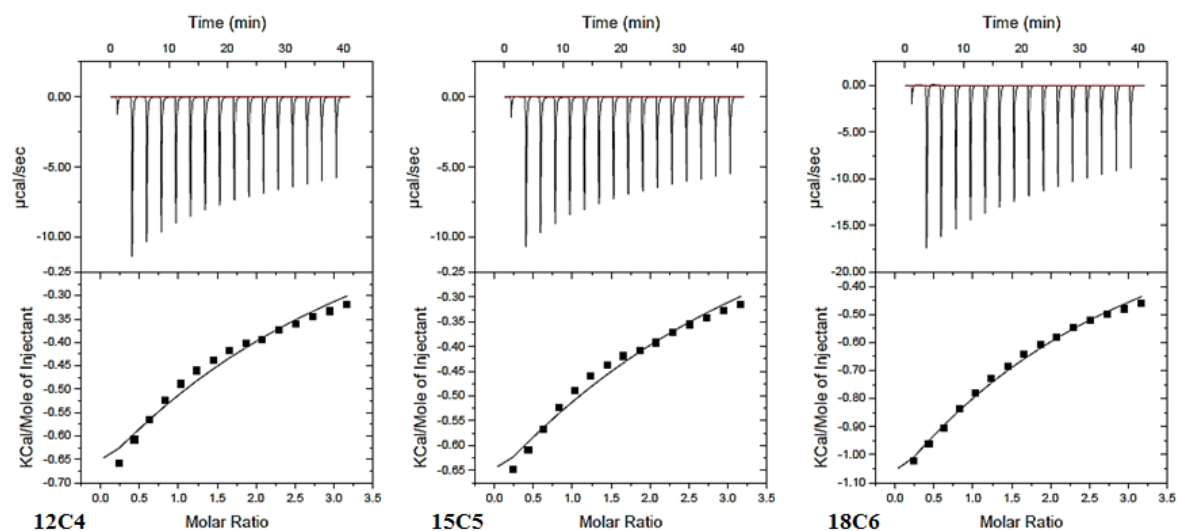


Figure 2 Isotherms for Ca^{2+} titration of 5 mmol 12C4, 15C5 and 18C6 crown ether solutions titrated using 100 mmol CaCl_2 .

Measured values of enthalpy (ΔH), stoichiometry (N), binding affinity (K_b) and entropy (ΔS) from this analysis are shown in **Table 2**

Table 2 ITC analysis at $\text{pH } 7.4 \pm 0.2$ of 12C4, 15C5 and 18C6 crown ethers titrated with CaCl_2 .

Chelator in	CaCl_2 in	Stoichiometry	Binding affinity	ΔH	ΔS
10 mM MES	10 mM MES	[N]	[K_b] (M^{-1})	(kJ mol^{-1})	($\text{J mol}^{-1} \text{deg}^{-1}$)
12C4 (5mM)	100 mM	1.99 ± 0.06	4.47 ± 1.37	-2.50 ± 0.22	-0.89 ± 0.18
15C5 (5mM)	100 mM	2.43 ± 0.03	4.36 ± 1.02	-1.84 ± 0.06	1.32 ± 0.22
18C6 (5mM)	100 mM	1.60 ± 0.07	4.20 ± 3.20	-4.11 ± 0.24	-6.35 ± 0.91

There is a strong interest of researchers in the studies of complexation between crown ethers and various cations.⁴¹⁻⁴³ A number of studies has been published on the analysis of complexation thermodynamics in these systems. Many of these studies were conducted using organic solvents, which is not relevant to interactions in biological systems. There is also lack of studies of the complexation between crown ethers and calcium ions in aqueous media. Izatt et al⁴⁴ have used calorimetric titration procedure to study the 1:1 reactions between 15-crown-5 and 18-crown-6 and several uni- and bivalent cations at 25 °C in aqueous solutions. However, they did not record any measurable heat effects for the complexation of 15C5 with Ca²⁺ and observed only very weak interactions between 18C6 and Ca²⁺. Solov'ev et al⁴⁵ later used solution calorimetry and ⁴³Ca NMR spectroscopy to study the thermodynamics of the complexation of 18C6 with calcium chloride and nitrate in aqueous solutions in a broad range of concentrations. They reported ΔH and ΔS values of CaCl₂ complexation with 18C6 to be $-9.44 \pm 2.18 \text{ kJ mol}^{-1}$ and $-22.9 \pm 7.3 \text{ J mol}^{-1} \text{ K}^{-1}$, which is greater compared to the values observed in our work. The discrepancy between our results and the data reported by Solov'ev et al⁴⁵ could be due to the difference in the calorimetric equipment and protocols used in both studies.

Ca²⁺ extraction from bovine cornea using crown ethers

Crown ethers are known for their ability to sequester metal ions, the efficiency of this effect depends on many factors, for example, cavity size, enthalpy and pH.^{39,40} Smaller metal ions deform the chelate ring to make interactions stronger between the metal ion and oxygen atoms within the molecule, whilst larger ions reside close to but outside the cavity.¹⁵ Here, the ability of 12C4, 15C5 and 18C6 crown ether solutions to extract Ca²⁺ ions from bovine cornea was investigated using atomic absorption spectrometry. Using the 'whole eye method',²⁸ 1 mL of 20

mg mL⁻¹ solutions of 12C4, 15C5 and 18C6 crown ethers in PBS at pH 7.4 ± 0.2 were exposed to an area of bovine cornea (1.54 ± 0.22 cm²) for 3 hours. Three fresh eyes were used for each crown ether solution and after exposure the solutions were recovered, centrifuged for 10 minutes at 10000 rpm and the supernatant was diluted in 0.25 w/v aqueous LaCl₃ solution for AAS analysis. This investigation has shown that PBS has the ability to absorb Ca²⁺ ions and this is likely to be due to dissolving soluble mucins from the ocular surface. Crown ethers are able to sequester Ca²⁺ from the cornea above this ‘background’ level.⁴⁶ **Figure 3** shows differences in calcium content of solutions before corneal exposure compared to the same solutions after exposure to the cornea. All formulations show a net increase in Ca²⁺ concentration at the end of this experiment and the rank order of calcium sequestering performance from bovine cornea compared to PBS is; PBS (54.67 ± 7.04 ppm) < 12C4** (62.58 ± 1.10 ppm) < 15C5** (69.42 ± 0.65 ppm) < 18C6* (81.39 ± 1.38 ppm). * *P* < 0.05, ** *P* < 0.01, *** *P* < 0.001, one-way ANOVA, *n* = 3.

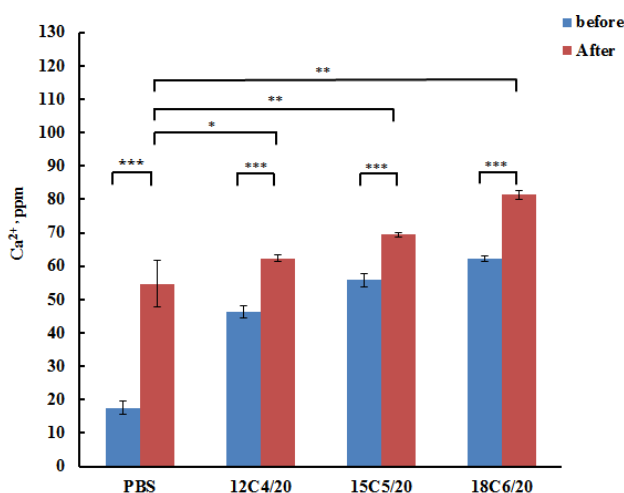


Figure 3 Ca^{2+} concentration in solutions of crown ethers (20 mg mL^{-1}) in PBS before and after 3 hours exposure to bovine cornea. * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$, one way ANOVA, $n = 3$.

Effect of crown ethers on permeability of riboflavin through bovine cornea

In vitro studies using Franz diffusion cells were carried out to investigate any permeability enhancement of riboflavin using crown ethers. The receiving chamber was filled with PBS at physiological pH (7.4) and 1 mL of each crown ether solution in PBS incorporating 0.08 mg mL^{-1} riboflavin was added to the epithelial side of the cornea. $200 \mu\text{L}$ aliquots were taken for HPLC analysis every 60 minutes for 240 minutes. Experiments were carried out in triplicate and analysis was carried out at the time of sampling to prevent sample degradation. Results are reported as the mean \pm standard deviation. Statistical analysis by ANOVA was applied and P values < 0.05 were considered significant. **Figure 4a** shows the overlaid riboflavin permeability profiles for crown ethers at 1 mg mL^{-1} , **Figure 4b** shows the graphs for crown ethers at 30 mg mL^{-1} , error bars have not been included for clarity. The same profiles are shown individually with error bars in supporting information (**Figure S1**). The results show that 12C4, 15C5 and 18C6 crown ethers at 1 mg mL^{-1} all afford a moderate enhancement in riboflavin permeability across bovine cornea to 22 ± 6 , 19 ± 7 and $14 \pm 4 \text{ ng mL}^{-1}$ at 240 minutes respectively compared to riboflavin in PBS which is $8 \pm 2 \text{ ng mL}^{-1}$, whilst at 30 mg mL^{-1} they offer a significant enhancement at 62 ± 23 , 35 ± 4 and $33 \pm 7 \text{ ng mL}^{-1}$ respectively. There is no significant difference in riboflavin permeability enhancement between the different crown ethers except for the difference between 12C4 and 18C6 at 30 mg mL^{-1} .

Apparent permeability and steady state flux were calculated using **Equation 3** and the results are given in **Table 3**.

Table 3 Steady state flux and apparent permeability of riboflavin through bovine cornea in PBS with and without crown ether.

Solution	Steady-state flux, ($\mu\text{mol min}^{-1}$)	P_{app} ($\text{cm s}^{-1} \times 10^{-3}$)
PBS	0.0478	1.945
12C4 1 mg mL ⁻¹	0.1208	6.138
15C5 1 mg mL ⁻¹	0.1074	5.457
18C6 1 mg mL ⁻¹	0.0753	3.826
12C4 30 mg mL ⁻¹	0.341	17.326
15C5 30 mg mL ⁻¹	0.1961	9.964
18C6 30 mg mL ⁻¹	0.1811	9.202

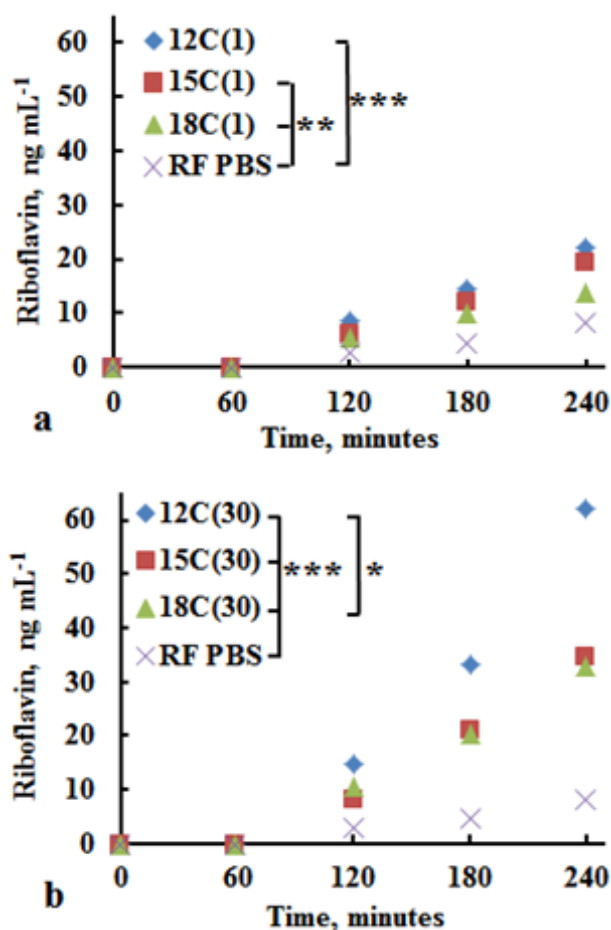


Figure 4 Permeability profiles for riboflavin in crown ether / PBS solutions through bovine cornea. Crown ethers at 1 mg mL⁻¹ (a), 30 mg mL⁻¹ (b) * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$, one way ANOVA, $n = 3$.

Comparing riboflavin permeability enhancing performance between crown ethers and polyaminocarboxylic acids at the same concentration (1 mg mL⁻¹) and with riboflavin concentration at 0.08 mg mL⁻¹ it has been shown that crown ethers have superior permeability enhancing properties (**Table 4**). The smallest crown ether molecular variant offered the best performance.

Table 4 Bovine cornea permeation of riboflavin using polyaminocarboxylic acids and crown ethers.

Enhancer, 1 mg mL ⁻¹	Riboflavin, μmol
EDTA	0.032 \pm 0.007
EGTA	0.035 \pm 0.004
EDDS	0.025 \pm 0.010
12C4	0.059 \pm 0.016
15C5	0.052 \pm 0.018
18C6	0.036 \pm 0.011

Effect of crown ethers on riboflavin penetration into bovine cornea

When treating corneal disorders such as keratoconus, it is essential that riboflavin is taken up by the stroma where UVA collagen cross-linking is facilitated.⁵ Therefore, crown ether mediated riboflavin transport into the cornea was evaluated.

Corneas from the above diffusion studies were trimmed to exclude limbal and scleral tissue. Riboflavin was extracted using absolute ethanol with subsequent analysis using HPLC. It was found that all the crown ethers investigated enhanced corneal absorption of riboflavin significantly greater than riboflavin in PBS alone. At 1 mg mL⁻¹ there was an increasing concentration of riboflavin extract from the corneas; 0.470 \pm 0.003 ng mg⁻¹ for 12C4,*** 0.930 \pm 0.145 ng mg⁻¹ for 15C5*** and 1.450 \pm 0.182 ng mg⁻¹ for 18C6.** At 30 mg mL⁻¹ there was a further increase in riboflavin extract, however the trend reversed with the highest concentration for 12C4 at 1.790 \pm 0.245 ng mg⁻¹***, reducing to 1.510 \pm 0.164 ng mg⁻¹ for 15C5*** and to

$1.00 \pm 0.1975 \text{ ng mg}^{-1}$ for 18C6.*** **Table 5** lists the amounts of riboflavin extracted from bovine corneas after exposure to PBS with and without crown ether after 4 hours exposure. * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$, one way ANOVA, $n = 3$.

Table 5 Riboflavin extracted from treated corneas after 4 hours exposure, ng mg^{-1} .

Crown ether solution in PBS with 0.08 mg mL^{-1} riboflavin	Riboflavin, ng mg^{-1} cornea
PBS	0.060 ± 0.001
12C4 1 mg mL^{-1}	0.470 ± 0.003 ***
15C5 1 mg mL^{-1}	0.930 ± 0.145 ***
18C6 1 mg mL^{-1}	1.450 ± 0.182 **
12C4 30 mg mL^{-1}	1.790 ± 0.245 ***
15C5 30 mg mL^{-1}	1.510 ± 0.164 ***
18C6 30 mg mL^{-1}	1.000 ± 0.198 ***

* $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$, one way ANOVA, $n = 3$.

Toxicological investigation

Epithelial damage is linked to corneal opacity and this phenomenon can be indicative of a substances ocular toxicity. **Figure 5** shows that the three different crown ethers, 12C4, 15C5 and 18C6, produce a similar level of epithelial change, and increasing the concentration from 1 mg

mL⁻¹ to 30 mg mL⁻¹ does not increase induced opacity. The level of epithelial damage caused by crown ethers was similar to that caused by the various concentrations of the BAC compounds and was much lower compared with the positive controls, NaOH 0.5 M and 1.0 M, which display a high level of corneal opacity due to alkali burning. BAC is often used in ocular formulations in concentrations up to 0.02% to act as a penetration enhancer and preservative.⁴⁷ At higher concentration BAC is known to be an irritant and toxic.⁴⁸

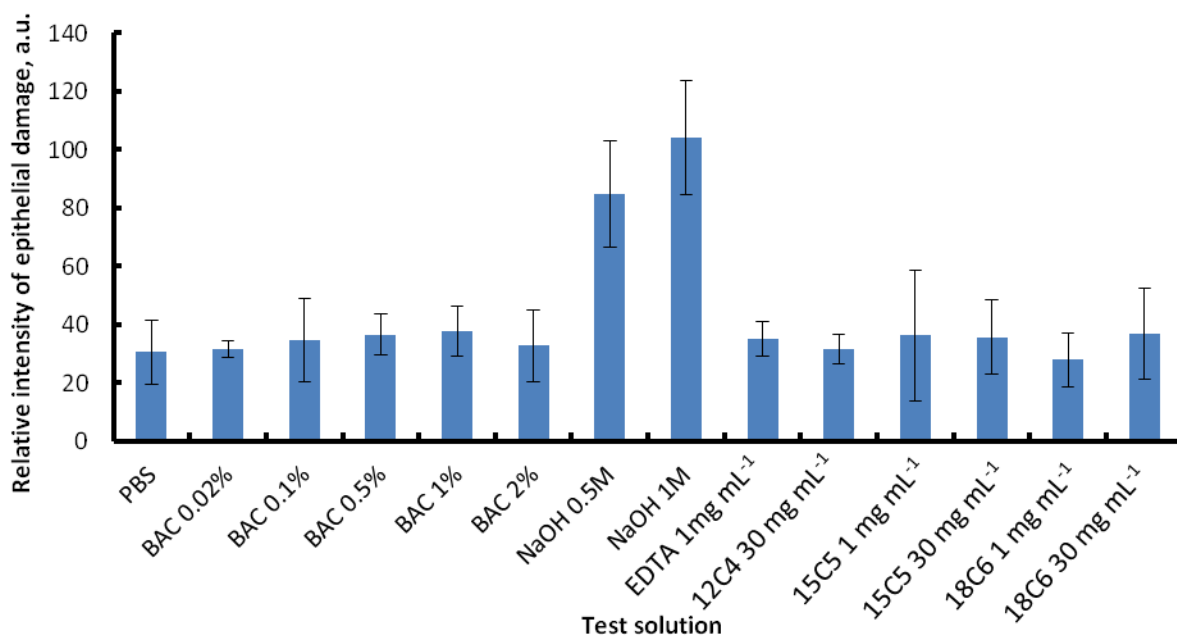


Figure 5 Relative intensity of epithelial damage caused by PBS (negative control), BAC 0.02%, BAC 0.1%, BAC 0.5%, BAC 1%, BAC 2%, NaOH 0.5M, (positive control) NaOH 1M, positive control) EDTA 1mg mL⁻¹, 12C4 30g mL⁻¹, 15C5 1 and 30 mg mL⁻¹ and 18C6 1 and 30 mg mL⁻¹. No significant difference between all tested compounds except for the positive controls which showed a significantly damaging effect on bovine cornea epithelia.*** *** $P < 0.001$, one way ANOVA, $n = 3$.

Crown ethers display ionophoretic properties in cell membranes and behave similarly to natural ionophores, i.e. valinomycin, a cyclicdepsipeptide antibiotic.^{22,49} Therefore, their toxic effect is thought to be due to penetration of the cellular bilayer membrane.⁵⁰ By applying these compounds to the cornea, epithelial disruption allows for permeation of fluorescein dye. **Figure 6** shows that the fluorescent intensity of epithelial surfaces treated with the crown ethers is comparable to corneas treated with BAC 1% and 2%.* High permeation of the fluorescein dye shows that if the permeability enhancer was to be used in conjunction with a therapeutic compound such as riboflavin in eye drop formulations, it would afford assisted transport into the cornea and could eliminate the need for invasive epithelial removal. Comparing crown ethers with BAC in the concentrations shown suggests they appear to be more toxic than BAC at the accepted level (0.02%)* used in many eye drop formulations, but less toxic than BAC concentrations >0.1% and EDTA at 1mg mL⁻¹, especially for the 12C4 variant. The positive controls 0.5 M NaOH and 1.0 M NaOH were significantly more toxic than all other compounds tested.*** * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$, one way ANOVA, n = 3.

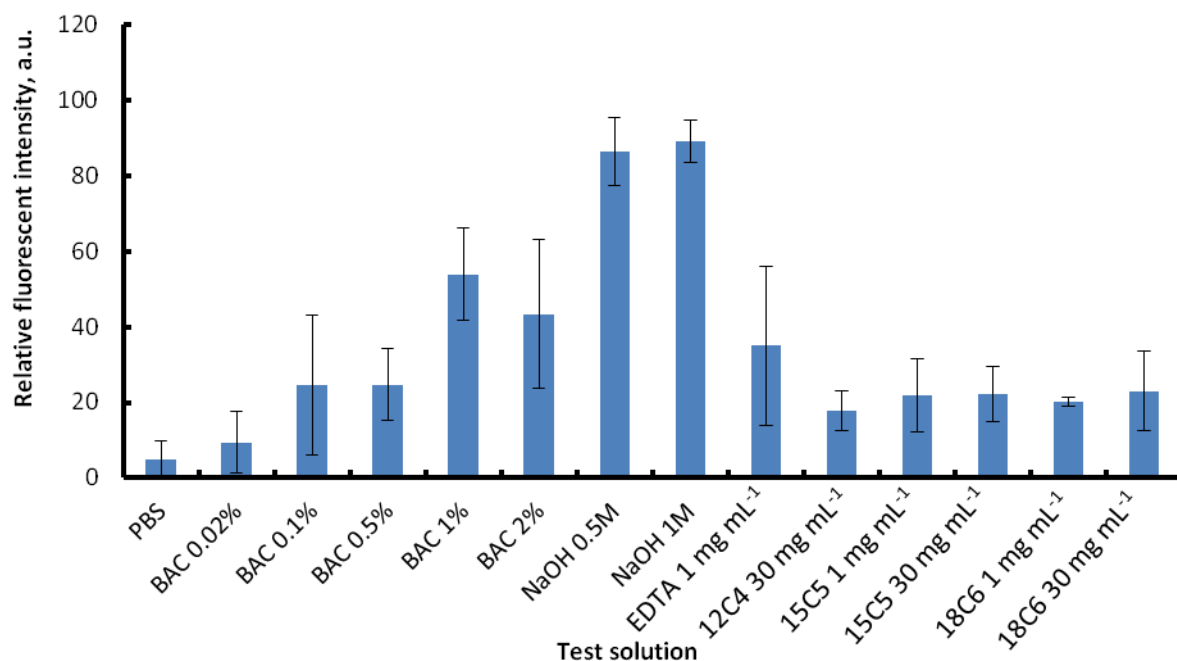


Figure 6 Fluorescent intensity of epithelial surface pre-treated with PBS, BAC 0.02% to 2.0%, EDTA 1 mg mL⁻¹, NaOH 0.5 M and 1.0 M and crown ether between 1 and 30 mg mL⁻¹, followed with fluorescein sodium staining

In vivo experiments

In vivo experiments were conducted in Wistar rats (n=3) to test ocular penetration of riboflavin using 0.08 mg mL⁻¹ drug formulations with and without 30 mg mL⁻¹ 12C4, the crown ether that demonstrated the best penetration enhancement performance in vitro. 2 mL of the drug formulations were instilled into both eyes gradually within 40 min (**Figure S2**). This timing was chosen to ensure the practicality of working with live animals and also to keep it relatively close to the drug administration procedure used clinically (30 min⁵).

Unfortunately, the results of these in vivo experiments did not show any statistically significant penetration enhancement effect with 30 mg mL⁻¹ 12C4: the amounts of riboflavin extracted from

the eyes after the application of the formulations with and without 12C4 were 0.3889 ± 0.0998 and $0.4855 \pm 0.1702 \mu\text{g g}^{-1}$, respectively, and the difference between these values is not statistically significant ($p > 0.05$).

Additional experiments were performed to evaluate the effect of riboflavin formulations with and without 30 mg mL^{-1} 12C4 on the epithelial morphology of rat corneas. **Figure 7** shows the histological images of rat corneas, following in vivo administration of $1 \text{ mL } 0.08 \text{ mg mL}^{-1}$ riboflavin solutions with and without 30 mg mL^{-1} 12C4 during 40 mins. A comparison of the corneal morphology allows conclusions that the use of formulation containing 30 mg mL^{-1} 12C4 does not lead to any serious epithelial disruption. The epithelial cells remain intact and tightly attached to the stroma. Previously, we have reported the disruptive effects of cyclodextrins²⁸ and chelating agents¹⁵ on the bovine corneas in vitro. However, we did not observe any similar disruptive effects in vivo.

Unfortunately, in vivo experiments did not provide any evidence for penetration enhancement effects caused by 12C4.

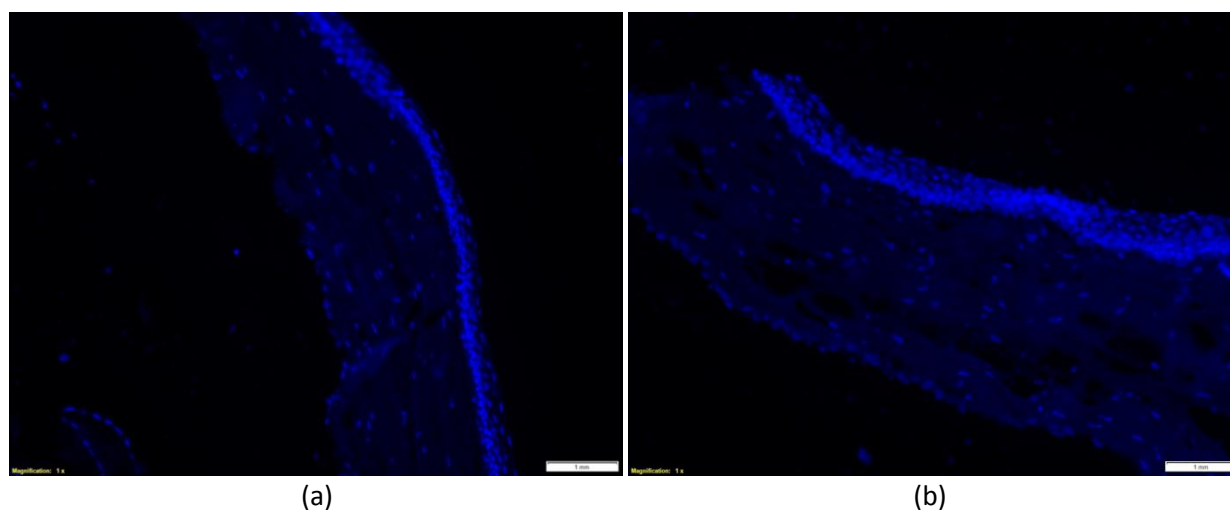


Figure 7. Histology of rat corneas following in vivo administration of 1 mL 0.08 mg mL⁻¹ riboflavin solution without (a) and with (b) 30 mg mL⁻¹ 12C4 during 40 mins. Scale bar is 100 µm.

The possible reason for this lack of in vitro – in vivo correlation is the dynamic nature of live corneal surfaces that are continuously washed with a tear fluid. During in vitro experiments the riboflavin formulations containing crown ethers as penetration enhancers clearly exhibited better drug penetration because of the static nature of bovine corneas, giving a possibility for their prolonged contact with a biological surface. In vivo the situation is very much different and the enhancer is quickly washed off the ocular surface. To test this hypothesis, we have conducted additional experiments on fluorescein retention on rat's cornea in vivo. 1 mg mL⁻¹ sodium fluorescein solution was administered on rat's cornea and UV light was briefly shone into their eye to improve its detection, which under these conditions showed green fluorescence. Digital images were taken at different time intervals and some exemplary images are shown in **Figure 8**.

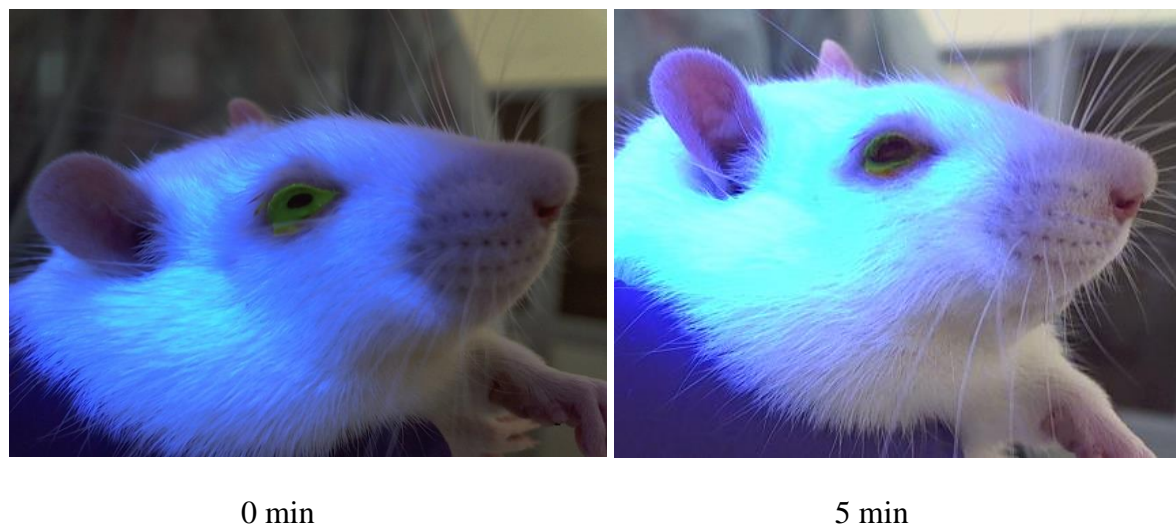


Figure 8. Retention of 1 mg mL⁻¹ sodium fluorescein on rat's cornea *in vivo*. UV light was shone to the eye to facilitate the detection of green fluorescence from sodium fluorescein.

It is clearly seen that sodium fluorescein is quickly washed off the corneal surface even within 5 minutes after ocular administration. This correlates well with our recent report on *in vivo* retention of fluorescein on rabbit corneas *in vivo*: non-viscous formulations containing fluorescein stayed on the corneal surfaces only for a few minutes.⁵¹ This lack of *in vitro* – *in vivo* correlation clearly highlights the need for further *in vivo* experiments in this area. The majority of *in vitro* models used to study drug retention / penetration into the ocular tissues are quite limited and cannot fully mimic the complex physiology of the ocular environment.

Conclusions

Crown ethers were investigated for their riboflavin solubility enhancing properties which could improve the drugs bioavailability. It was found that 12C4 at 1 mg mL⁻¹ offered a slight reduction to the solubility of riboflavin whilst 15C5 and 18C6 at 1 mg mL⁻¹ and all the investigated crown ethers at higher concentrations offered significant enhancement to riboflavin solubility, thereby increasing its availability for use in ocular drug formulations. Permeability enhancement of bovine corneas was investigated based on crown ethers ability to sequester metal ions, namely Ca²⁺, and on their ionophoric properties which could potentially improve drug transport across the physical barriers of the cornea. Riboflavin transport through bovine cornea was enhanced by all the crown ethers investigated and it was found that 12C4 was the most efficient at both concentrations tested (1 mg mL⁻¹ and 30 mg mL⁻¹), this could be due the size differences of the crown ether / drug complex. Crown ethers in PBS were found to significantly improve Ca²⁺ extraction from corneal epithelia compared to PBS alone; therefore they have the ability to

loosen Ca^{2+} dependant tight junctions in the epithelial membrane. The permeability enhancing properties of crown ethers were shown to be superior compared to polyaminocarboxylic acids investigated in our previous study,¹⁵ however, it is concluded that crown ethers ionophoric properties enhance riboflavin permeability more than their Ca^{2+} sequestering properties. Further experiments determined that all the crown ether solutions investigated were efficient at delivering riboflavin into the corneal stroma and this is necessary for effective treatment following established UV 'A' induced collagen cross linking for the treatment of keratoconus and other conditions of the cornea. Crown ethers are novel compounds which have not previously been investigated for ocular drug delivery prior to this study, therefore an assessment of potential toxicological implications of using crown ethers in ocular formulations was carried out and their toxicity was found to be of a similar level to BAC which is used as a preservative and penetration enhancer for eye drop medication. Crown ethers at 1 mg mL^{-1} and 30 mg mL^{-1} were shown to have lower epithelial toxicity than EDTA at 1 mg mL^{-1} . This study has shown that crown ethers have an important role in development of ocular medications for improvement of drug solubility, enhanced drug penetration into the cornea and potential to eliminate the need for epithelial removal for treatment of corneal disorders.

Unfortunately, in vivo experiments performed in rats did not establish any significant enhancement in riboflavin permeation into the eye mediated with 30 mg mL^{-1} 12C4. The reason for this lack of permeability enhancement is the dynamic nature of live ocular tissue that is continuously washed with a tear fluid. Additional experiments with fluorescein confirmed that retention on the surface of the cornea in vivo is poor. Future research may look at the application of crown ethers in combination with mucoadhesive polymers to enhance both the drug permeability and pre-corneal retention. Another important finding from these experiments is a

clear need for conducting in vivo experiments to evaluate the efficiency of a formulation to enhance corneal permeability of drugs. This work clearly demonstrated that experiments with ex vivo corneas could provide valuable information about drug permeation and permeability enhancement properties of different agents; however, this information is limited and cannot always predict the behaviour of a drug delivery system in vivo.

Further studies will be required to evaluate the potential of crown ethers to enhance corneal permeability for other drugs. Additionally, the studies where crown ethers are combined with mucoadhesive polymers to enhance drug permeation and to improve pre-corneal retention will be of interest. Our recent study of timolol maleate formulations⁵² demonstrated that the combination of permeability enhancers with some mucoadhesive polymers could potentially inhibit drug permeation through the cornea despite the improvements in pre-corneal retention, which indicates that there is still lack of understanding of permeability enhancement effects in multicomponent drug formulations.

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SUPPORTING INFORMATION

The Supporting Information is available free of charge on the ACS Publications website at xx. It includes images and numerical data from toxicological experiments, individual permeability profiles and image from in vivo experiments.

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